

# Artificial Matrices With High-Sulfated Glycosaminoglycans and Collagen Are Anti-Inflammatory and Pro-Osteogenic for Human Mesenchymal Stromal Cells

Ute Hempel,<sup>1\*</sup> Claudia Matthäus,<sup>1</sup> Carolin Preissler,<sup>1</sup> Stephanie Möller,<sup>2</sup> Vera Hintze,<sup>3</sup> and Peter Dieter<sup>1</sup>

<sup>1</sup>*Institute of Physiological Chemistry, Carl Gustav Carus Faculty of Medicine, TU Dresden, Fiedlerstrasse 42 D-01307, Dresden, Germany*

<sup>2</sup>*INNOVENT e. V., Biomaterials Department, Prüssingstrasse 27 B D-07745, Jena, Germany*

<sup>3</sup>*Max Bergmann Center of Biomaterials, Technical University Dresden, Budapester Straße 27 D-01069, Dresden, Germany*

## ABSTRACT

Bone healing has been described to be most efficient if the early inflammatory phase is resolved timely. When the inflammation elevates or is permanently established, bone healing becomes impaired and, moreover, bone destruction often takes place. Systemic disorders such as diabetes and bone diseases like arthritis and osteoporosis are associated with sustained inflammation and delayed bone healing. One goal of biomaterial research is the development of materials/surface modifications which support the healing process by inhibiting the inflammatory bone erosion and suppressing pro-inflammatory mediators and by that promoting the bone repair process. In the present study, the influence of artificial extracellular matrices (aECM) on the interleukin (IL)-1 $\beta$ -induced pro-inflammatory response of human mesenchymal stromal cells (hMSC) was studied. hMSC cultured on aECM composed of collagen I and high-sulfated glycosaminoglycan (GAG) derivatives did not secrete IL-6, IL-8, monocyte chemoattractant protein-1, and prostaglandin E<sub>2</sub> in response to IL-1 $\beta$ . The activation and nuclear translocation of nuclear factor  $\kappa$ Bp65 induced by IL-1 $\beta$ , tumor necrosis factor- $\alpha$  or lipopolysaccharide was abrogated. Furthermore, these aECM promoted the osteogenic differentiation of hMSC as determined by an increased activity of tissue non-specific alkaline phosphatase (TNAP); however, the aECM had no effect on the IL-1 $\beta$ -induced TNAP activity. These data suggest that aECM with high-sulfated GAG derivatives suppress the formation of pro-inflammatory mediators and simultaneously promote the osteogenic differentiation of hMSC. Therefore, these aECM might offer an interesting approach as material/surface modification supporting the bone healing process. *J. Cell. Biochem.* 115: 1561–1571, 2014. © 2014 Wiley Periodicals, Inc.

**KEY WORDS:** EXTRACELLULAR MATRIX; GLYCOSAMINOGLYCANS; INFLAMMATION; MESENCHYMAL STROMAL CELLS; OSTEOGENIC DIFFERENTIATION; PROSTAGLANDINS

Abbreviations: (a)ECM, (artificial) extracellular matrix; BM, basal medium; col, collagen; COX, cyclooxygenase; CS, chondroitin sulfate; DAPI, 4',6-diamidino-2-phenylindole; Dex, dexamethasone; DKK-1, dickkopf-related protein-1; DMEM, Dulbecco's minimal essential medium; DS<sub>S</sub>, degree of sulfation per disaccharide repeating unit; ELISA, enzyme-linked immunosorbent assay; ERK, extracellular-regulated kinase; GAG(s), glycosaminoglycan(s); HA, hyaluronan; hMSC, human mesenchymal stromal cells; IKK, I $\kappa$ B kinase; IL, interleukin; LPS, lipopolysaccharide; MCP-1, (CCL2) monocyte chemoattractant protein-1; MTS, (3-(4,5-dimethylthiazol-2-yl)-5-(3-carboxymethoxyphenyl)-2-(4-sulfophenyl)-2H-tetrazolium); NF $\kappa$ B, nuclear factor  $\kappa$ B; OM/D, osteogenic differentiation medium; PBS, phosphate-buffered saline; PGE<sub>2</sub>, prostaglandin E<sub>2</sub>; sCS3, high-sulfated CS (DS<sub>S</sub> ~3); sHA3, high-sulfated hyaluronan (DS<sub>S</sub> ~3); STAT, signal transducer and activator of transcription; TCPS, tissue culture polystyrene; TNAP, tissue non-specific alkaline phosphatase; TNF- $\alpha$ , tumor necrosis factor- $\alpha$ .

Current address of Claudia Matthäus is Max Delbrück Center for Molecular Medicine, Developmental Neurobiology, Robert-Rössle-Str. 10, 13092 Berlin, Germany.

\*Correspondence to: Ute Hempel, Institute of Physiological Chemistry, Carl Gustav Carus Faculty of Medicine, Technische Universität Dresden, Fiedlerstrasse 42, D-01307 Dresden, Germany. E-mail: ute.hempel@tu-dresden.de

Manuscript Received: 23 January 2014; Manuscript Accepted: 4 April 2014

Accepted manuscript online in Wiley Online Library (wileyonlinelibrary.com): 7 April 2014

DOI 10.1002/jcb.24814 • © 2014 Wiley Periodicals, Inc.

**B**one healing includes an inflammatory phase followed by bone formation and remodeling processes [Claes et al., 2012]. The inflammatory reaction is induced immediately after tissue damage by fracture, surgical intervention or by introducing an implant. Inflammatory cells such as granulocytes, monocytes and macrophages become activated and secrete various pro-inflammatory mediators which influence the differentiation/function of bone-forming osteoblasts, bone-resorbing osteoclasts and their mesenchymal and hematopoietic precursor cells. When exposed to an inflammatory environment, osteoblasts and mesenchymal stromal cells (MSC) themselves secrete various pro-inflammatory mediators and by that contribute to the sustainment of inflammation or to the repair process [Tomchuck et al., 2008]. A moderate, controlled and quickly resolved inflammatory reaction is essential for physiological bone healing; for example, anti-inflammatory drugs are known to have a negative effect on bone healing when they are applied in the early phase of inflammation [Pietrogrande et al., 2011]. Otherwise, the over-exposition of bones and joints with pro-inflammatory mediators, systemic and long-term chronic inflammation causes impaired or decelerated bone healing or even more bone/joint destructions as known from osteo- or rheumatoid arthritis [Blackwell et al., 2010; Bastian et al., 2011; Kapoor et al., 2011; Thomas and Puleo, 2011]. Yang et al. [2007] described a delayed bone healing in interleukin (IL)-6 knockout mice.

The switch from the positive effect of inflammation in early/initial bone healing to the negative effect of hyper-inflammation or chronic inflammation is associated with the number and subpopulation of inflammatory cells and secreted mediators [Bastian et al., 2011]. The release of pro-inflammatory mediators leads to the inhibition of osteoblast function partly by inhibition of the extracellular-regulated kinase (ERK1/2), activation of signal transducers and activators of transcription (STAT), activation of the nuclear factor (NF) $\kappa$ B, and up-regulation of the Dickkopf-related protein (DKK1) and sclerostin [Redlich and Smolen, 2012]. NF $\kappa$ B transcription factor is activated by a plethora of stimuli and mediates varied gene expression programs [Oeckinghaus et al., 2011]. Pro-inflammatory mediators such as IL-1 $\beta$ , tumor necrosis factor (TNF)- $\alpha$  and lipopolysaccharide (LPS), each interacting with its specific receptor, lead to the activation/phosphorylation of the I $\kappa$ B kinase (IKK) complex consisting of the catalytically active subunits IKK $\alpha$ , IKK $\beta$ , and the regulatory subunit IKK $\gamma$ . The catalytically active IKK subunit phosphorylate I $\kappa$ B in the NF $\kappa$ B/I $\kappa$ B complex which results in release of the NF $\kappa$ B dimer from the complex, ubiquitinylation and proteasomal degradation of phospho-I $\kappa$ B, and translocation of NF $\kappa$ Bp65/NF $\kappa$ Bp50 heterodimer into the nucleus (canonical pathway) where it regulates the transcription of genes responsible for pro-inflammatory mediators [Ben-Neriah and Karin, 2011].

Glycosaminoglycans (GAGs) are multifunctional components of the pericellular and extracellular matrix (ECM). They consist of repeating disaccharide units, for example, of D-glucuronic acid- $\beta$ (1 $\rightarrow$ 3)-N-acetyl-D-galactosamine-4-sulfate- $\beta$ (1 $\rightarrow$ 4) (chondroitin sulfate) or of D-glucuronic acid- $\beta$ (1 $\rightarrow$ 3)-N-acetyl-D-glucosamine- $\beta$ (1 $\rightarrow$ 4) (hyaluronan). Sulfated negatively charged GAGs like chondroitin sulfate, dermatan sulfate or heparan sulfate are mostly covalently bound to core proteins forming proteoglycans which are part of membrane-spanning syndecans, GPI-anchored glypicans or

associated to ECM as aggrecan, versican, biglycan, or decorin. The non-sulfated, negatively charged hyaluronan can form a backbone for several proteoglycans and is able to bind enormous amounts of water, to swell and function in several tissues as a space holder and immune modulator. GAGs interact with many cations and proteins and are able to modulate the bioavailability of growth factors, cytokines and chemokines [Macri et al., 2007]. GAGs act as co-receptors for many growth factors; for example, the association of basic fibroblast growth factor (bFGF) with heparan sulfate is important for the interaction of bFGF with its membrane receptor [Gallagher and Turnbull, 1992]. Natural sulfated glycosaminoglycans (GAGs), for example, chondroitin sulfate (CS), seem to have beneficial effects on the pathophysiology of osteoarthritis; they reduced blood markers of inflammation and the activity of destructive proteases like matrixmetalloproteinases, diminished pain and improved the function of the affected joint [Martell-Pelletier et al., 2010; Volpi, 2011; Hochberg et al., 2013].

Synthetically sulfated hyaluronan derivatives (sHA) were at first characterized and described as antithrombogenic substances [Magnani et al., 1996; Chen et al., 1997; Magnani et al., 1998] and inhibitors of TNF- $\alpha$  [Chang et al., 1994]. A pro-osteogenic effect of sulfated hyaluronan derivatives was described by Nagahata et al. [2004] with rat calvarial cells who demonstrated that the substances induced the formation of cell aggregates with increased activity of tissue non-specific alkaline phosphatase (TNAP). aECM composed of collagen (col) and synthetically high-sulfated GAG derivatives increased the osteogenic differentiation of hMSC [Hempel et al., 2012a]. These aECM are known to influence many cellular functions of hMSC such as cell-matrix interactions, signal transductions pathways and endocytosis [Büttner et al., 2013; Kliemt et al., 2013] and led to a considerable inhibition of osteoclast function [Salbach et al., 2012a].

In the present study, the influence of aECM containing col, the natural GAGs CS and HA as well as high-sulfated GAG derivatives on the response of hMSC to inflammatory stimuli was investigated. Particularly the effect on the formation of pro-inflammatory mediators [IL-6, IL-8, monocyte-chemoattractant protein-1 (MCP-1), and prostaglandin E<sub>2</sub> (PGE<sub>2</sub>)] and the involvement of cyclooxygenase-2 (COX-2) and NF $\kappa$ B were analyzed. To examine the influence of aECM on the osteogenic differentiation of hMSC in response to IL-1 $\beta$ , the activity of TNAP was determined.

## MATERIALS AND METHODS

Cell culture plastic material (TCPS) was from Greiner (Frickenhausen, Germany) and Nunc (Wiesbaden, Germany). Dulbecco's minimum essential medium (DMEM), trypsin, penicillin/streptomycin antibiotics, and phosphate buffered saline (PBS) were purchased from Biochrom (Berlin, Germany). Fetal calf serum was from BioWest (via Th.Geyer, Hamburg, Germany). LPS (*Salmonella minnesota*) and the other biochemical reagents were from Sigma (Taufkirchen, Germany). For the determination of protein concentration the RotiQuant assay from Roth (Karlsruhe, Germany) was used. For the determination of IL-1 $\beta$ , IL-6, IL-8, and MCP-1 concentration, DuoSet enzyme-linked immunosorbent assay (ELISA) Development Kits (R&D Systems, Wiesbaden, Germany) were used. For the determination of COX-2

protein, total COX-2 cell-based ELISA kit (R&D Systems) was used. The determination of NF $\kappa$ B activation was performed with the NF $\kappa$ Bp65 TransAM<sup>TM</sup> Kit (Active Motif, La Hulpe, Belgium). Human IL-1 $\beta$  and hTNF- $\alpha$  were purchased from Peprotech (Hamburg, Germany). Rat tail collagen I was from BD Bioscience (Heidelberg, Germany). CS [from *bovine trachea*, mixture of CSA(70)/CSC(30)] was obtained from Sigma and HA (from *Streptococcus*) was obtained from Aqua Biochem (Dessau, Germany). High-sulfated chondroitin sulfate (sCS3, degree of sulfation per disaccharide (DS<sub>S</sub>)  $\sim$ 3) derivative and high-sulfated hyaluronan (sHA3, DS<sub>S</sub>  $\sim$  3) derivative were synthesized as described earlier [Hempel et al., 2012b].

#### PREPARATION AND CHARACTERIZATION OF ARTIFICIAL EXTRACELLULAR MATRICES (aECM)

aECM were prepared from collagen I and CS, HA or the high sulfated GAG derivatives sCS3 and sHA3 and characterized as described earlier [Hempel et al., 2012a,b]. In brief, 1 mg collagen I was dissolved in 1 ml of ice cold 10 mM acetic acid and was mixed with an equal volume of 1 mg GAG derivative/ml dissolved in ice cold double concentrated fibrillogenesis buffer (50 mM sodium dihydrogenphosphate, 11 mM potassium dihydrogenphosphate, pH 7.4). Two hundred twenty microliters of the collagen I/sGAG derivative mixture per cm<sup>2</sup> were placed onto tissue culture polystyrene plates (TCPS). Fibrillogenesis was performed overnight at 37°C. The resulting aECM was air-dried, washed two times with 1 ml deionized, sterile water and air-dried again. Before the cell culture experiments, an additional washing step with sterile PBS for 1 h at 37°C was performed.

#### ISOLATION AND CULTIVATION OF HUMAN MESENCHYMAL STROMAL CELLS (hMSC)

The hMSC were isolated from bone marrow aspirates, obtained from Caucasian donors (average age 32  $\pm$  7 years, mixed gender) at the Bone Marrow Transplantation Center of the University Hospital Dresden, and were characterized as described [Oswald et al., 2004]. The donors were informed about the procedures and gave their full consent. The study was approved by the local ethics commission (ethic vote No. EK114042009). Four hMSC preparations were chosen for the experiments according prior characterization of osteogenic differentiation capacity and according the characteristic: "similar basal TNAP activity in passage 1." hMSC preparations of individual donors were not pooled. The cells were used in passage 2–4. 7,000 hMSC/cm<sup>2</sup> were plated in Dulbecco's minimal essential medium (DMEM) with 10% heat-inactivated fetal calf serum and 10,000 IE penicillin/10,000  $\mu$ g streptomycin/ml (=basal medium, BM) onto tissue culture polystyrene (TCPS) or aECM-coated TCPS.

For the determination of released pro-inflammatory mediators (IL-6, IL-8, MCP1, PGE<sub>2</sub>), analysis of gene expression (*nf $\kappa$ B* and *cox-2*), COX-2 protein content and the MTS assay, sub-confluent hMSC (sub-confluence was seen 72 h after plating) were serum-starved in DMEM supplemented with 10,000 IE penicillin/10,000  $\mu$ g streptomycin/ml for 24 h and treated afterwards with IL-1 $\beta$  (10 ng/ml) for 24 h. For the determination of NF $\kappa$ B activation, sub-confluent hMSC were serum-starved for 24 h and treated afterwards with IL-1 $\beta$  (10 ng/ml), TNF- $\alpha$  (10 ng/ml) or LPS (1  $\mu$ g/ml), respectively, for 1 h.

For the determination of TNAP activity and mineral accumulation, hMSC were treated 24 h after plating in BM with 10 ng IL-1 $\beta$ /

ml. At day 4 after plating, hMSC were cultured in BM or osteogenic differentiation medium (BM with 10 mM  $\beta$ -glycerophosphate, 300  $\mu$ M ascorbic acid, 10 nM dexamethasone = OM/D); thereafter, the medium was changed twice per week and 10 ng IL-1 $\beta$ /ml was added with each medium change. At day 11 after plating, the activity of TNAP was determined. At day 22 after plating, the calcium phosphate deposition was quantified.

#### CONCENTRATION OF IL-6, IL-8, MCP-1, AND PGE<sub>2</sub>

Twenty-four hours after IL-1 $\beta$  treatment, conditioned medium of hMSC was collected and analyzed for the concentration of IL-6, IL-8, and MCP-1 using DuoSet ELISA Development Kits according to manufacturer's instructions. PGE<sub>2</sub> concentration was determined with a competitive ELISA as described earlier [Dieter et al., 1999].

#### IL-1 $\beta$ RECOVERY

aECM were incubated with 10 ng IL-1 $\beta$ /ml in BM for 1 and 24 h at 37°C. The concentration of IL-1 $\beta$  in the conditioned medium was determined with human IL-1 $\beta$  DuoSet ELISA Development Kit according to manufacturer's instructions.

#### METABOLIC ACTIVITY

Metabolic activity of hMSC was determined by MTS assay (Cell Titer96 AQueous One Solution Proliferation Assay) (Promega, Mannheim, Germany). For the analysis, conditioned medium was replaced by fresh medium containing 10% of MTS dye solution. After 2 h of incubation at 37°C in a humidified CO<sub>2</sub> incubator, 100  $\mu$ l cellular medium was transferred into a 96-well plate and the absorbance of the formed MTS formazan dye was measured photometrically at 490 nm.

#### ACTIVATION, TRANSLOCATION, AND EXPRESSION OF NF $\kappa$ B

**Activation:** One hour after treatment with IL-1 $\beta$ , TNF- $\alpha$ , and LPS, hMSC were washed twice with PBS and lysed according to manufacturer's instructions for TransAM<sup>TM</sup> NF $\kappa$ Bp65 assay. Protein concentration of the lysate was determined by Rotiquant<sup>®</sup> assay (Roth GmbH, Karlsruhe, Germany) and calculated from a linear calibration curve ( $r = 0.9967$ ) obtained with bovine serum albumin. Four micrograms of cellular protein were applied to the TransAM<sup>TM</sup> NF $\kappa$ Bp65 assay.

**Translocation:** For visualization of phospho-NF $\kappa$ B, hMSC were treated with IL-1 $\beta$  for 1 h, washed afterwards with PBS and fixed with 4% paraformaldehyde (w/v) in PBS for 10 min. After permeabilization with 0.1% Triton X-100 in PBS for 20 min, non-specific binding sites were blocked with 1% bovine serum albumin (w/v) in PBS containing 0.05% Tween-20. The cells were incubated for 1 h with rabbit-anti-human phospho-NF $\kappa$ Bp65-Ser536 monoclonal antibody (Cell Signalling, Frankfurt a. M., Germany, no. #3031) dissolved in PBS, containing 1% bovine serum albumin and 0.05% Tween-20. After washing with PBS, cells were incubated with blocking buffer for 10 min again. AlexaFluor-568-conjugated goat-anti-rabbit polyclonal antibody (Invitrogen, Karlsruhe, Germany, no. A11011) dissolved in PBS containing 1% bovine serum albumin and 0.05% Tween-20, was used as a secondary antibody. Nuclei were stained with 0.2  $\mu$ g 4',6-diamidino-2-phenylindole (DAPI)/ml PBS for 10 min at 25°C. After staining, the cells were embedded in Mowiol

TABLE I. Primer Pairs Used for Real Time PCR

Gene	Accession no.	Forward primer	Reverse primer	Binding position	Product length (bp)	Product identity (%) <sup>a</sup>
<i>actin</i> <sup>b</sup>	NM001101.3	aatgtggccgaggactttgattgc	ttaggatggcaaggactctctgt	1,414–1,508	95	100
<i>gapdh</i> <sup>b</sup>	NM002046.3	tgcttcgatgggtgtaacca	tgatggcatggactgtggatcat	563–718	156	97
<i>nfkB</i> <sup>b</sup>	NM003998.3	accctgacctgtcctatttg	agctcttttcccgatctcc	985–1,054	70	100
<i>cox-2</i> <sup>b</sup>	NM000963.1	caaatccttctgttcccacca	tgcactgtgttgaggatgggttc	187–358	172	98

<sup>a</sup>Determined by sequencing of amplified DNA products.

<sup>b</sup>Genes: *actin*,  $\beta$ -actin; *gapdh*, glyceraldehyde-3-phosphate dehydrogenase; *nfkB*, nuclear factor  $\kappa$ B; *cox-2*, cyclooxygenase-2.

4-88 (Sigma) and visualized using an AxioPhot fluorescence microscope (Carl Zeiss, Oberkochen, Germany). The fluorescence signals were detected using the following filters: excitation 546 nm and emission 590 nm for AlexaFluor-568 and excitation 365 nm and emission 420 nm for DAPI. Digital images were obtained with an AxioCam MRm camera (Carl Zeiss) by using AxioVision software release 4.6 (Carl Zeiss).

**Gene expression:** For the analysis of *nfkB* gene expression, RNA was prepared from cell lysates after 24 h of treatment with IL-1 $\beta$  using RNeasy Mini Kit (Qiagen, Hilden Germany). cDNA was synthesized using the QuantiTect Reverse Transcription Kit (Qiagen) including a DNA digestion step. Real-time PCR reactions were performed using RotorGene PG-3000 PCR machine (Corbett, Wasserburg, Germany) with the RotorGene SYBR Green PCR Kit (Qiagen). After the initial activation step at 95°C for 5 min, 50 PCR cycles (denaturation at 95°C for 5 s; annealing and synthesis at 60°C for 10 s) were carried out. Primers were constructed by use of Universal Probe Library (Roche, Mannheim Germany) (see Table I for detailed information) and synthesized by Eurofines MWG Operon (Ebersberg, Germany). The same single stranded cDNA was used to analyze the expression of the gene of interest and the house-keeping genes *beta-actin* and *gapdh*. The relative expression values were calculated with both *beta-actin* and *gapdh* using the comparative quantification method of the RotorGene software release 6.0. The values are normalized to hMSC in BM on TCPS.

#### COX-2 GENE EXPRESSION AND PROTEIN

Gene expression of *cox-2* was analyzed as described above (see Table I for detailed information). COX-2 protein content was quantified with the total COX-2 cell-based ELISA kit (KCB4198; R&D systems) according to manufacturer's instructions. The fluorescence signal was determined using a fluorescence plate reader (FluoroStar Optima, BMG Labtech, Ortenberg, Germany) with excitation at 540 nm and emission at 600 nm for COX-2 and with excitation at 360 nm and emission at 450 nm for GAPDH. COX-2 amount was normalized to GAPDH amount.

#### TNAP ACTIVITY

TNAP activity was determined in cell lysates (lysis buffer: 1.5 M Tris-HCl (pH 10), 1 mM ZnCl<sub>2</sub>, 1 mM MgCl<sub>2</sub> and 1% Triton X-100) with *p*-nitrophenylphosphate as a substrate as described previously [Hempel et al., 2012a] and calculated from a linear calibration curve ( $r = 0.9979$ ) prepared with *p*-nitrophenol. Specific TNAP activity is given in mU/mg protein. Protein concentration of the lysate was determined as described above.

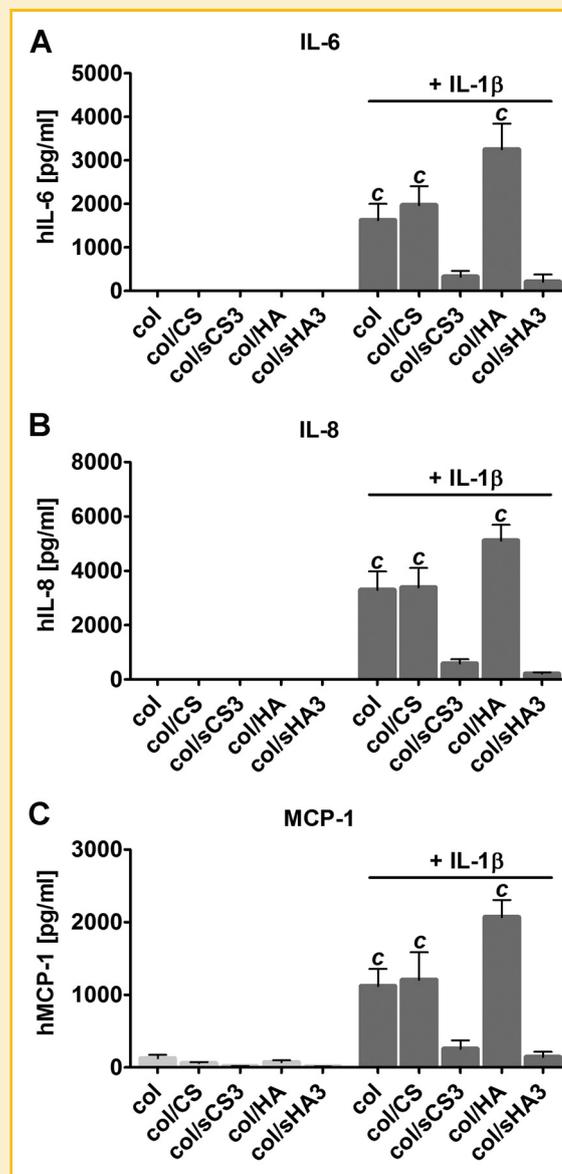


Fig. 1. Formation of IL-6, IL-8, and MCP-1. hMSC (7,000 cells/cm<sup>2</sup>) were cultured on aECM composed of collagen and CS, sCS3, HA, and sHA3 in BM. At day 3 after plating, hMSC were serum-starved for 24 h. Then the cells were treated with 10 ng IL-1 $\beta$ /ml for 24 h. The concentration of IL-6 (A), IL-8 (B), and MCP-1 (C) was determined in conditioned medium by ELISA. The data are presented as mean  $\pm$  SEM,  $n = 4$ . Significant differences of IL-1 $\beta$  treatment versus untreated cells comparing the same aECM were indicated as c ( $P < 0.001$ ).

## CALCIUM PHOSPHATE DEPOSITION

Calcium phosphate deposition was quantified with the calcium and the phosphorus kit (both from Greiner Diagnostics, Bahlingen, Germany) as previously described [Hempel et al., 2012a]. Cell layers were washed with PBS, dried and incubated with 0.5 M HCl at 4°C for 24 h. Calcium and phosphate content in the lysates were quantified photometrically with cresolphthalein complexone at 570 nm and ammonium molybdate at 340 nm, respectively. Both, calcium and phosphate content ( $\mu\text{mol}/\text{cm}^2$ ) was calculated from linear calibration curves ( $r > 0.99$ ). Cell-free aECM samples (control) were treated in the same way as aECM with cultured cells and analyzed for calcium and phosphate.

## STATISTICAL ANALYSIS

The experiments were performed with hMSC from four different donors, each in triplicate. The results are presented as mean  $\pm$  standard error of the mean (SEM). Statistical significance was analyzed with GraphPad Prism 5.04 software (Statcon, Witzenhhausen, Germany) by two-way ANOVA analysis with Bonferroni's post-test. Significant differences of IL-1 $\beta$  treated cells versus untreated cells comparing the same aECM were indicated with italic characters (*a* for  $P < 0.05$ , and *c* for  $P < 0.001$ ). Significant differences of GAG-aECM versus col were indicated by hash mark (# for  $P < 0.001$ ).

## RESULTS

For all in vitro experiments, MSC were cultured onto five different aECM. To evaluate directly the effect of IL-1 $\beta$ , TNF- $\alpha$ , and LPS on NF $\kappa$ B activation, serum-starved hMSC were treated for 1 h with these stimuli (pre-tests showed maximum NF $\kappa$ B activation at this time point). To evaluate directly the effect of IL-1 $\beta$  on the formation of IL-6, IL-8, MCP-1, and PGE<sub>2</sub> as well as on expression and protein level of COX-2, and on expression of *nfkB*, serum-starved hMSC were treated for 24 h (pre-tests showed maxima for these parameters). To evaluate the effect of IL-1 $\beta$  on osteogenic differentiation, hMSC were cultured either in BM or in OM/D until day 11 (early

differentiation phase indicated by increasing TNAP activity) and day 22 (late differentiation phase indicated by increasing calcium phosphate accumulation) with permanent addition of IL-1 $\beta$ .

## INFLUENCE OF aECM AND IL-1 $\beta$ ON THE FORMATION OF IL-6, IL-8, AND MCP-1

hMSC which were cultured on different aECM, treated with IL-1 $\beta$  for 24 h and analyzed for the formation of IL-6 (Fig. 1A), IL-8 (Fig. 1B), and MCP-1 (Fig. 1C). Untreated cells showed no or only a marginal release of IL-6, IL-8, and MCP-1 on all aECM. IL-1 $\beta$  induced a strong significant ( $P < 0.001$ ) increase of IL-6, IL-8, and MCP-1 in hMSC on col, col/CS, and col/HA; in contrast, only a weak not significant formation of IL-6, IL-8, and MCP-1 was induced in hMSC cultured on the high-sulfated aECM col/sCS3 and col/sHA3.

To exclude that the aECM or treatment with IL-1 $\beta$  had an effect on the metabolic activity of the cells, the MTS assay was performed. The metabolic activity of cells was neither affected by the aECM or the addition of IL-1 $\beta$  (Fig. 2A). To exclude that IL-1 $\beta$  was trapped by the aECM with high-sulfated GAG derivatives, the recovery of IL-1 $\beta$  after 1 and 24 h of incubation with the aECM at 37°C was analyzed. After 1 h  $96.7 \pm 1.8\%$  and after 24 h  $90.9 \pm 1.4\%$  of the added IL-1 $\beta$  was found in the conditioned medium independently on the aECM (Fig. 2B) indicating that all aECM did not markedly bind IL-1 $\beta$ .

## INFLUENCE OF aECM AND IL-1 $\beta$ ON THE ACTIVATION, GENE EXPRESSION, AND TRANSLOCATION OF NF $\kappa$ B

The transcription factor NF $\kappa$ B is activated in response to inflammatory stimuli and regulates the formation of certain pro-inflammatory mediators such as IL-6, IL-8, and MCP-1 [Novack, 2011]. For the analysis of NF $\kappa$ B activation an ELISA for measurement of NF $\kappa$ Bp65-binding to its consensus DNA site was used. Untreated cells showed on all aECM a marginal and comparable activation of NF $\kappa$ Bp65. IL-1 $\beta$ , TNF- $\alpha$  and LPS induced an about 5–10-fold significant ( $P < 0.001$ ) activation of NF $\kappa$ Bp65 in hMSC on col, col/CS, and col/HA but only a small not significant activation on the high-sulfated aECM col/sCS3 and col/sHA3

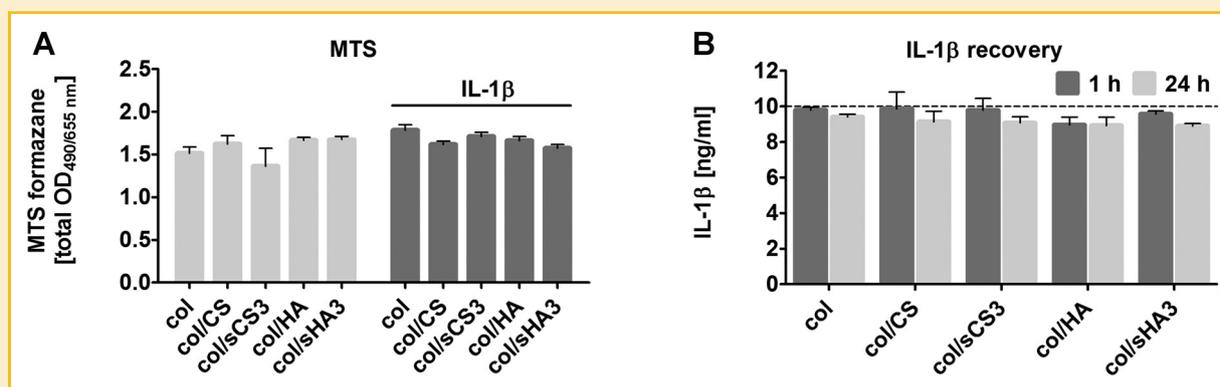
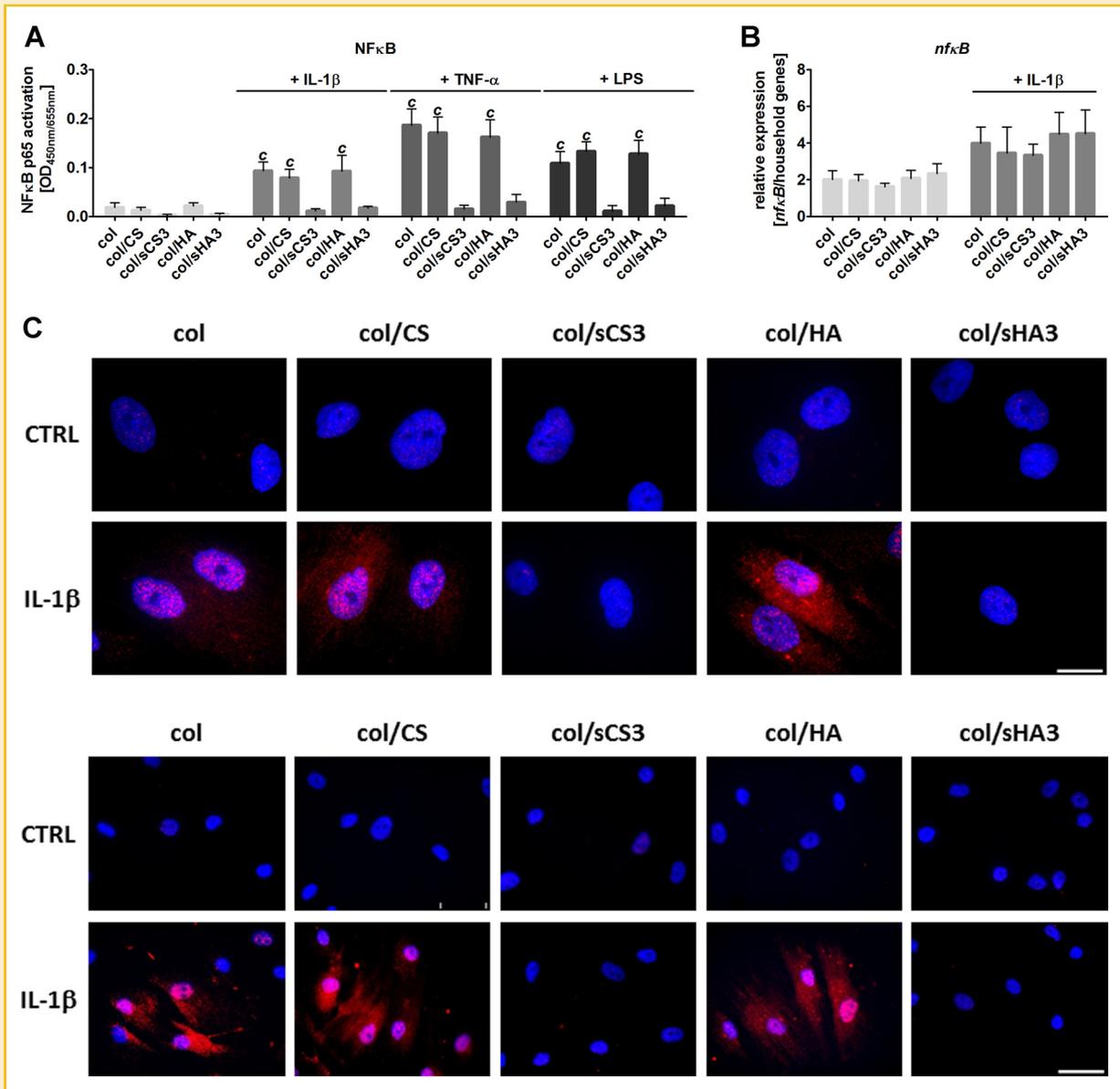


Fig. 2. Metabolic activity and IL-1 $\beta$  recovery. hMSC ( $7,000 \text{ cells}/\text{cm}^2$ ) were cultured on aECM composed of collagen and CS, sCS3, HA, and sHA3. At day 3 after plating, hMSC were serum-starved for 24 h. Then the cells were treated with 10 ng IL-1 $\beta$ /ml for 24 h. The metabolic activity was measured by MTS assay (A). Data presented as mean  $\pm$  SEM,  $n = 4$ . B: aECM were incubated at 37°C for 1 and 24 h with 10 ng IL-1 $\beta$ /ml in BM. IL-1 $\beta$  concentration in conditioned medium was determined by ELISA. The recovery of IL-1 $\beta$  is shown; the dotted line represents the initial IL-1 $\beta$  concentration,  $n = 3$ .



**Fig. 3.** Activation, expression, and translocation of NFκB. hMSC (7,000 cells/cm<sup>2</sup>) were cultured on aECM composed of collagen and CS, sCS3, HA, and sHA3 in BM. At day 3 after plating, hMSC were serum-starved for 24 h. **A:** Activation: hMSC were treated with 10 ng IL-1β/ml, 10 ng TNF-α/ml and 1 μg LPS/ml for 1 h and analyzed for NFκB DNA-binding activity using the TransAM™ NFκBp65 assay. Data presented as mean ± SEM, n = 4. Significant differences of treated cells versus untreated cells comparing the same aECM were indicated as c (P < 0.001). **B:** Gene expression: hMSC were treated with 10 ng IL-1β/ml for 24 h. The expression of *nfκB* was assessed by real time PCR and is related to expression of *beta-actin* and *gapdh*. The data are presented as mean ± SEM, n = 4. **C:** Translocation: hMSC were treated with 10 ng IL-1β/ml for 1 h and analyzed for phospho-NFκBp65-Ser-536. hMSC were fixed and stained with rabbit anti-phospho-NFκBp65-Ser536-monoclonal antibody/AlexaFluor-568 anti-rabbit IgG (red fluorescence) and DAPI for nuclei (blue fluorescence). Typical images are shown; scale bar = 50 μm.

(Fig. 3A). The aECM had no effect on the basal or IL-1β-induced expression of *nfκB* (Fig. 3B). IL-1β increased slightly but not significantly the expression of *nfκB*.

IL-1β induces the phosphorylation and translocation of NFκBp65 into the nucleus [Perkins, 2006]. Here, similar results were found for IL-1β stimulated hMSC on col, col/CS, and col/HA where phospho-NFκBp65-Ser536 was found cytosolic and co-localized with the nucleus; however, in hMSC on the high-sulfated col/sCS3 and col/

sHA3 no phospho-NFκBp65-Ser536 could be detected after IL-1β treatment (Fig. 3C).

#### INFLUENCE OF aECM AND IL-1β ON THE COX-2 GENE EXPRESSION, COX-2 PROTEIN, AND PGE<sub>2</sub> FORMATION

NFκB is involved in the IL-1β-induced expression of COX-2 and the COX-2 mediated formation of PGE<sub>2</sub> [Nakao et al., 2002; Hirata et al., 2009]. IL-1β induced a significant (P < 0.001) expression of

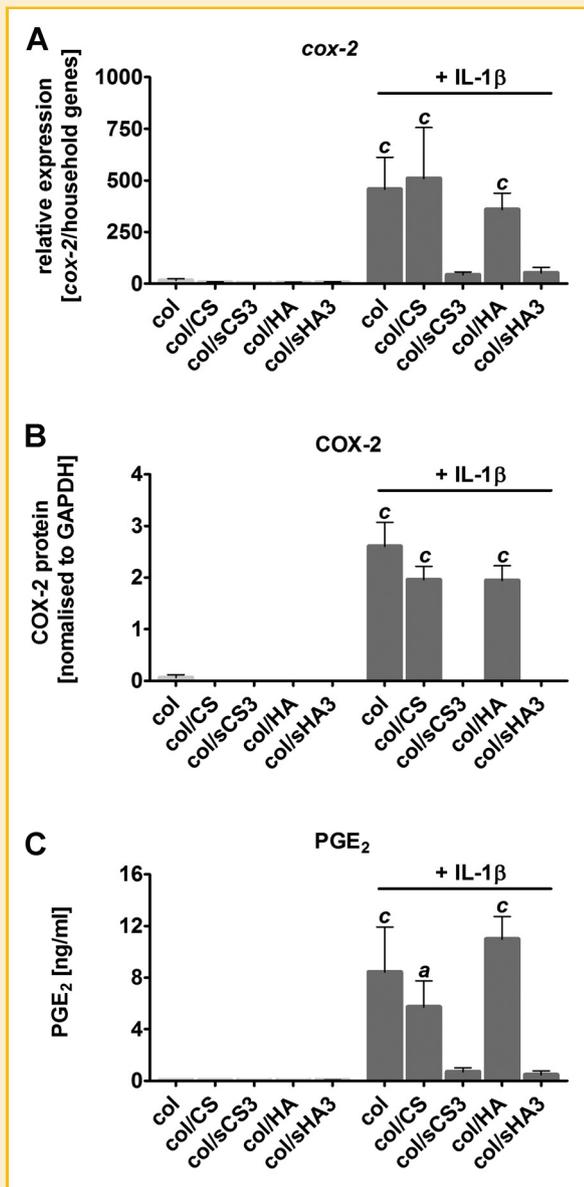


Fig. 4. Expression of COX-2 and PGE<sub>2</sub> formation. hMSC (7,000 cells/cm<sup>2</sup>) were cultured on aECM composed of collagen and CS, sCS3, HA, and sHA3 in BM. At day 3 after plating, hMSC were serum-starved for 24 h. A: Gene expression: Cells were treated with 10 ng IL-1β/ml for 24 h. The expression of *cox-2* was assessed by real time PCR and is related to expression of *beta-actin* and *gapdh*. B: COX-2 protein content: The amount of COX-2 protein was assessed by total COX-2 cell-based ELISA kit and related to GAPDH protein content in the same cell lysate. C: PGE<sub>2</sub> formation: PGE<sub>2</sub> concentration in the conditioned medium was determined by ELISA (C). The data are presented as mean ± SEM, n = 4. Significant differences of IL-1β treatment versus untreated cells comparing the same aECM were indicated as a ( $P < 0.05$ ) and c ( $P < 0.001$ ).

*cox-2* (Fig. 4A), a significant ( $P < 0.001$ ) increase of COX-2 protein (Fig. 4B) and in consequence a significant ( $P < 0.001$  for col and col/HA;  $P < 0.05$  for col/CS) formation of PGE<sub>2</sub> (Fig. 4C) in hMSC on col, col/CS, and col/HA whereas no or only a marginal response could be measured in hMSC on the high-sulfated col/sCS3 and col/sHA3.

## INFLUENCE OF aECM AND IL-1β ON TNAP ACTIVITY AND CALCIUM PHOSPHATE DEPOSITION

An increase of the TNAP activity is often used as a marker for osteogenic differentiation of MSC [Pittenger, 2008]. Here, hMSC in BM (undifferentiated cells, Fig. 5A) or OM/D (differentiated cells, Fig. 5B) showed at day 11 after plating a significant ( $P < 0.001$ ) two- to threefold increase of TNAP activity on the high-sulfated col/sCS3 and col/sHA3 compared to the other aECM. IL-1β induced an increased TNAP activity in hMSC in BM and OM/D on col, col/CS, and col/HA but did not increase TNAP activity in cells on col/sCS3 and col/sHA3 (Fig. 5A,B). Calcium phosphate deposition around the cells requires TNAP activity; the enzyme releases phosphate from the in vitro substrate β-glycerophosphate which lead to calcium phosphate deposition afterwards. Although hMSC in BM revealed TNAP activity, they did not deposit calcium phosphate because of the lack of β-glycerophosphate in the medium. At day 22 after plating, calcium phosphate deposition was seen in differentiated hMSC in OM/D with a significant ( $P < 0.001$ ) increase of calcium (Fig. 6A) and phosphate (Fig. 6B) on the high-sulfated col/sCS3 and col/sHA3 compared to the other aECM. IL-1β induced an increased calcium phosphate deposition in OM/D on col, col/CS, and col/HA but not on col/sCS3 and col/sHA3. These data are in line with results of TNAP activity. By plotting TNAP activity at day 11 versus calcium (Fig. 6C) and phosphate (Fig. 6D) at day 22, respectively, a linear correlation was seen. The ratio of the slopes,  $5.513 \pm 0.0906$  for calcium (Fig. 6C) and  $3.396 \pm 0.0576$  for phosphate (Fig. 6D), reflects the calcium to phosphate ratio and was with a value of 1.62 only slightly below the calcium to phosphate ratio in hydroxyapatite (1.67).

## DISCUSSION

Recently we showed that aECM composed of collagen and over-sulfated GAG derivatives had a pro-osteogenic effect on hMSC [Hempel et al., 2012a]. The present study focuses on the influence of those aECM on the IL-1β-induced inflammatory response of hMSC. The exposure of hMSC to an inflammatory environment might affect the osteogenic differentiation process of the cells and results in a subsequent impaired bone formation and bone healing processes [Bastian et al., 2011; Thomas and Puleo, 2011; Kapoor et al., 2011]. Here we demonstrated that aECM containing high-sulfated GAG derivatives were able to suppress IL-1β-induced pro-inflammatory responses of hMSC but enhanced simultaneously the osteogenic differentiation of the cells. aECM containing high-sulfated HA and CS derivatives inhibited the IL-1β-induced formation of IL-6, IL-8, and MCP-1. The aECM also suppressed the expression of *cox-2*, the amount of COX-2 protein and the formation of PGE<sub>2</sub>. Furthermore, the osteogenic differentiation of hMSC, as determined by the osteogenic marker TNAP and calcium phosphate deposition was enhanced by these aECM.

The inflammatory mediator IL-1β exerts its effects preferentially via activation and nuclear translocation of NFκB and also via activation of ERK1/2 and MAPK p38 [Oeckinghaus et al., 2011; Novack, 2011]; phosphorylated NFκBp65-Ser536, for example, has been shown to be essential for IL-1β induced IL-8 formation [Buss et al., 2004]. NFκB is discussed as a negative regulator of osteoblast

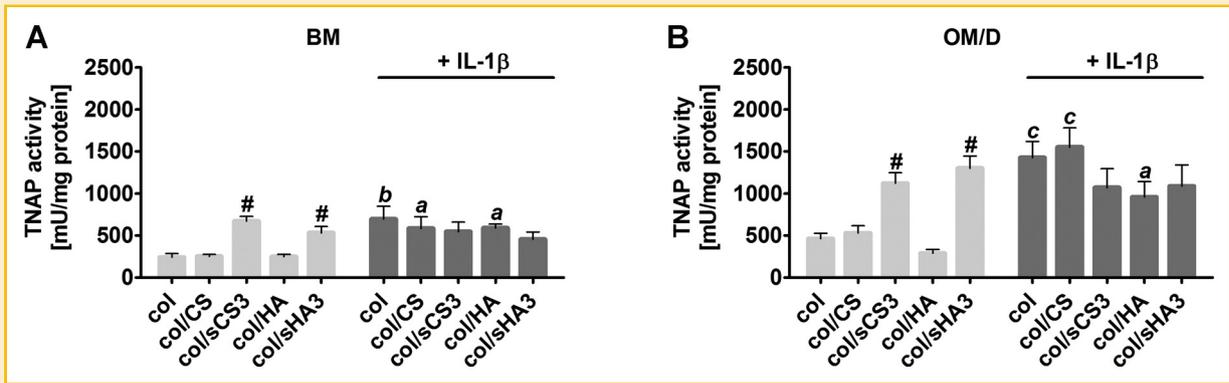


Fig. 5. Activity of TNAP. hMSC (7,000 cells/cm<sup>2</sup>) were cultured on aECM composed of collagen and CS, sCS3, HA, and sHA3 in BM. Twenty-four hours after plating hMSC were treated with 10 ng IL-1β/ml. From day 4 after plating, hMSC were either incubated in BM (A) or OM/D (B). The data are presented as mean ± SEM, n = 4. Significant differences of IL-1β treatment versus untreated cells comparing the same aECM were indicated as a (*P* < 0.05) and c (*P* < 0.001). Significant differences of GAG-aECM versus col were indicated as # (*P* < 0.001).

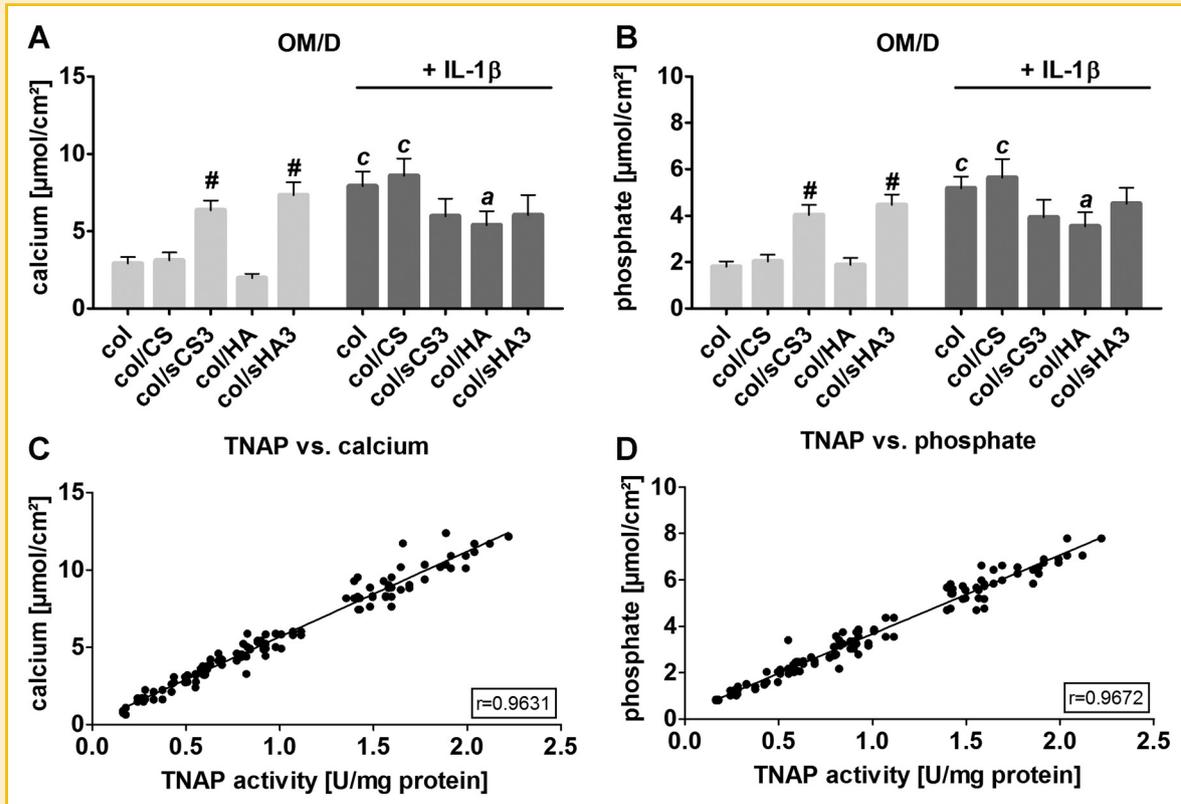


Fig. 6. Calcium phosphate deposition. hMSC (7,000 cells/cm<sup>2</sup>) were cultured on aECM composed of collagen and CS, sCS3, HA, and sHA3 in BM. Twenty-four hours after plating hMSC were treated with 10 ng IL-1β/ml. From day 4 after plating, hMSC were incubated BM or OM/D. At day 22 after plating, calcium and phosphate deposition by hMSC were determined complexometrically. The amount of calcium (A) and phosphate (B) deposited by hMSC in OM/D are presented as mean ± SEM, n = 4. Significant differences of IL-1β treatment versus untreated cells comparing the same aECM were indicated as a (*P* < 0.05) and c (*P* < 0.001). Significant differences of GAG-aECM versus col were indicated as # (*P* < 0.001). The values of TNAP activity at day 11 in OM/D were plotted against the corresponding calcium (C) and phosphate (D) values at day 22. The linear equation for TNAP versus calcium was  $y = (5.513 \pm 0.091)x + 0.1678 \pm 0.1014$  (C) and for TNAP versus phosphate  $y = (3.396 \pm 0.0576)x + 0.2769 \pm 0.0647$  (D); the correlation coefficients *r* are given in the plots.

differentiation [Novack, 2011]. An up-regulation of NF $\kappa$ B has been implicated in the pathogenesis of several inflammation-related bone diseases including osteoporosis, osteo- and rheumatic arthritis [Krum et al., 2010]. Chang et al. [2009] showed that activation of NF $\kappa$ B by pro-inflammatory mediators suppresses the expression of Fos-related antigen-1 which is important for bone formation and bone matrix deposition and that the inhibition of IKK/NF $\kappa$ B pathway in differentiating osteoblasts can prevent osteoporotic bone loss. Here we showed that IL-1 $\beta$  induced the activation and translocation of NF $\kappa$ B only in hMSC which were cultured on aECM containing col, col/CS, and col/HA. In hMSC which were cultured on aECM containing high-sulfated GAG derivatives, IL-1 $\beta$  did not lead to an activation of NF $\kappa$ B; moreover, these effect was independent of the stimulus and almost identical for stimulation with IL-1 $\beta$ , TNF- $\alpha$ , and LPS suggesting that the high-sulfated GAGs could directly interact with the activation and translocation process of NF $\kappa$ B. A recent study with macrophages demonstrated that such aECM with col and high-sulfated HA suppressed the activity of pro-inflammatory macrophages by abrogating NF $\kappa$ B activation indicating that the effect of these aECM is not only restricted to hMSC [Franz et al., 2013]. In several models of induced inflammation, natural chondroitin sulfate was reported to inhibit NF $\kappa$ B activation [Cañas et al., 2010]. Campo et al. [2008, 2009] showed that chondroitin sulfate prevents NF $\kappa$ B translocation in response to LPS and interferes with the NF $\kappa$ B activation pathway at the level of LPS receptor TLR-4. However, in rat calvarial osteoblasts [Kunze et al., 2010] and, as seen here in hMSC, chondroitin sulfate had no effect on the IL-1 $\beta$ -induced NF $\kappa$ B translocation.

PGE<sub>2</sub> has also been shown to be elevated in an inflammatory environment via NF $\kappa$ B-induced COX-2 [Nakao et al., 2002; Hirata et al., 2009]. The role of PGE<sub>2</sub> in bone formation/bone remodeling is ambiguous described: COX-2/PGE<sub>2</sub> are important for bone formation associated with bone healing, but are also associated with enhanced bone resorption induced by inflammation [Blackwell et al., 2010]. Chondroitin sulfate has been described to have a protective effect on osteoarthritis probably by inhibition of PGE<sub>2</sub> formation [Pecchi et al., 2012]. The high-sulfated GAG heparin as a modification of titanium-based biomaterials promoted the function of MG-63 osteoblast cell line and inhibited their inflammation response [Kim et al., 2011].

Although pro-inflammatory mediators lead to bone loss in many inflammation-associated diseases such as rheumatoid arthritis, osteoporosis, and diabetes, they are known to promote ectopic bone formation and calcification, for example, of the endothelium [Ding et al., 2009]. Therefore it was assumed that the induction of osteogenesis in response to inflammation could be an important prerequisite for bone healing and remodeling and also the reason of the excessive ossification as known from the inflammatory bone disease ankylosing spondylitis [Scotti et al., 2013]. Ding et al. [2009] demonstrated that IL-1 $\beta$  and TNF- $\alpha$  increased TNAP activity and calcium phosphate accumulation in vitro. TNF- $\alpha$ -induced osteogenic differentiation of hMSC, for example, involves the osteogenesis regulating mediators Wnt5a and Wnt10b [Lin et al., 2010; Briolay et al., 2013]. The effects of IL-1 $\beta$  were strongly dependent on the duration and the time point of exposition as well as on the differentiation status of the cells: when premature MSC were

exposed for a short time to IL-1 $\beta$ , an enhanced osteogenic differentiation was seen; in contrast, when osteoblasts received a long-term IL-1 $\beta$ -treatment, bone formation was rather inadequate [Lin et al., 2010]. Mumme et al. [2012] showed that IL-1 $\beta$  revealed its pro-inflammatory effect via NF $\kappa$ B whereas ERK1/2 was involved in the pro-osteogenic effect of IL-1 $\beta$ . The inhibition of NF $\kappa$ B promoted TNAP activity, expression of *col(1) $\alpha$ 1*, *osteocalcin*, and *osteopontin* in mesenchymal cells [Krum et al., 2010]. An enhanced osteogenic differentiation in periodontal ligament-derived MSC after inhibition of NF $\kappa$ B was described and explained by competition of NF $\kappa$ B-signaling with Wnt/ $\beta$ -catenin signaling [Chen et al., 2013].

It is described that sulfated GAGs act as important co-regulators of hMSC lineage commitment, osteoprogenitor cell fate and bone formation and exert their effects often by interaction with bone-related growth factors whose activity can be reduced or enhanced thereby [Macri et al., 2007]. The regenerative potential of several GAGs has been well described [Salbach et al., 2012b]. Recent studies provided evidence that synthetically over-sulfated GAG derivatives, containing additional sulfate groups per disaccharide repeating unit, enhanced osteogenic differentiation of hMSC as determined by an induction of TNAP and an enhancement of calcium phosphate deposition probably in a growth factor (e.g., bone morphogenetic protein)- and dexamethasone-independent manner [Hempel et al., 2012a; Büttner et al., 2013].

To summarize, the anti-inflammatory but pro-osteogenic reactions of hMSC cultured on aECM with high-sulfated GAG derivatives were probably induced by a suppression of the activation of NF $\kappa$ B mediated by high-sulfated GAG derivatives. Therefore, all downstream events such as nuclear translocation of NF $\kappa$ B and expression of pro-inflammatory mediators and *cox-2* were found to be abrogated. Whether the effects of the high-sulfated GAG derivatives were due to upstream-processes of the NF $\kappa$ B activation cascade (suggesting an intracellular mechanism) or to an interference with cell receptors (suggesting an extracellular mechanism) remain to be elucidated. In conclusion, synthetically over-sulfated GAG derivatives in combination with collagen I facilitate anti-inflammatory but pro-osteogenic reactions of hMSC and might be appropriate for tissue engineering approaches and biomaterial modifications.

## ACKNOWLEDGMENTS

The authors are very grateful to Professor Bornhäuser and colleagues from the stem cell lab of the University Hospital in Dresden for providing the human mesenchymal stromal cells. This work was supported by grant of Deutsche Forschungsgemeinschaft (SFB/TR67 projects B1, A2, and A3).

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